Chapter 6

Light-Activated Ion Pumps and Channels for Temporally Precise Optical Control of Activity in Genetically Targeted Neurons

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Abstract

The ability to turn on and off specific cell types and neural pathways in the brain, in a temporally precise fashion, has begun to enable the ability to test the sufficiency and necessity of particular neural activity patterns, and particular neural circuits, in the generation of normal and abnormal neural computations and behaviors by the brain. Over the last 5 years, a number of naturally occurring light-activated ion pumps and light-gated ion channels have been shown, upon genetic expression in specific neuron classes, to enable the voltage (and internal ionic composition) of those neurons to be controlled by light in a temporally precise fashion, without the need for chemical co-factors. In this chapter, we review three major classes of such genetically encoded "optogenetic" microbial opsins - light-gated ion channels such as channelrhodopsins, light-driven chloride pumps such as halorhodopsins, and light-driven proton pumps such as archaerhodopsins - that are in widespread use for mediating optical activation and silencing of neurons in species from C. elegans to nonhuman primate. We discuss the properties of these molecules - including their membrane expression, conductances, photocycle properties, ion selectivity, and action spectra - as well as genetic strategies for delivering these genes to neurons in different species, and hardware for performing light delivery in a diversity of settings. In the future, these molecules will not only continue to enable cutting-edge science, but may also support a new generation of optical prosthetics for treating brain disorders.

Key words: Photosensitive proteins, Retinal, Halorhodopsin, Arch, Light-sensitive chloride pump, Photocontrol of behavior, Channelrhodopsin, Archaerhodopsin, Optogenetics

1. Introduction

The ability to turn on and off specific cell types and neural pathways in the brain, in a temporally precise fashion, has begun to enable the ability to test the sufficiency and necessity of particular

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neural activity patterns, and particular neural circuits, in the generation of normal and abnormal neural computations and behaviors by the brain. Most electrophysiological and imaging experiments in neuroscience are correlative - comparing a neural signal observed in the brain, to a behavior or pathology. In contrast, the power to manipulate specific cells and circuits is opening up the ability to understand their causal roles in brain functions. Over the last 5 years, a number of naturally occurring light-activated ion pumps and light-activated ion channels have been shown, upon genetic expression in specific neuron classes, to enable the voltage (and internal ionic composition) of those neurons to be controlled by light in a temporally precise fashion. These molecules are microbial (type I) opsins, seven-transmembrane proteins naturally found in archaea, algae, fungi, and other species, and which possess light-driven electrogenic activity or lightgated ion pores. These molecules, when heterologously expressed in neurons or other cells, translocate ions across cell membranes in response to pulses of light of irradiances that are easily achievable with common laboratory microscopes, LEDs, and lasers. These molecules have begun to find widespread use in neuroscience, due to their ease of handling and use (each is a single gene, less than 1-kb long, encoding for a monolithic protein), their lack of need for chemical supplementation in many species (they utilize the naturally occurring chromophore all-trans retinal, which appears to occur at sufficient quantities in the mammalian nervous system), and their high speed of operation (they can respond within tens of microseconds to milliseconds, upon delivery of light, and shut off rapidly upon cessation of light, as needed for neuroscience experiments).

Three major classes of such "optogenetic" microbial opsins have been described to date. The first class, channelrhodopsins, is exemplified by the light-gated inwardly rectifying nonspecific cation channel channelrhodopsin-2 (ChR2) from the green algae Chlamydomonas reinhardtii (1), which, when expressed in neurons, can mediate sizeable currents up to 1,000 pA in response to millisecond-timescale pulses of blue light (2–5), thus enabling reliable spike trains to be elicited in ChR2-expressing neurons by blue light pulse trains (Fig. 1b). Several additional channelrhodopsins useful to biologists and bioengineers have been discovered or engineered, with faster or slower kinetics, red-shifted activation, and cell region-specific targeting, explored in detail below (6-10). The channel hodopsins have been used to activate neurons in neural circuits in animals from worms to monkeys, and have proven to be powerful and easy to use. The second class of microbial opsins utilized for biological control to date, halorhodopsins, is exemplified by the light-driven inwardly directed chloride pump halorhodopsin, from the archaeal species Natronomas pharaonis (Halo/NpHR/pHR; (11)), which, when



Fig. 1. Three classes of microbial opsins that enable optical neural activation and silencing tools. (a) Neuron expressing hChr2-mCherry (ai; bar, 20 μ m) and Halo-GFP (aii). (b) Poisson trains of spikes elicited by pulses of blue light (*blue dashes*), in two different neurons. (c) Light-driven spike blockade, demonstrated (*top*) for a representative hippocampal neuron, and (*bottom*) for a population of neurons (n=7). *I-injection*, neuronal firing induced by pulsed somatic current injection (300 pA, 4 ms). *Light*, hyperpolarization induced by periods of yellow light (*yellow dashes*). *I-injection + light*, yellow light drives Halo to block neuron spiking, leaving spikes elicited during periods of darkness intact. (a-c) Adapted from (3) and (12). (d) Photocurrents of Arch vs. Halo measured as a function of 575 ± 25 nm light irradiance (or effective light irradiance), in patch-clamped cultured neurons (n=4-16 neurons for each point), for low (i) and high (ii) light powers. The line is a single Hill fit to the data. (e) *Top*, Neural activity in a representative neuron before, during, and after 5 s of yellow-light illumination, shown as a spike raster plot (*top*) and as a histogram of instantaneous firing rate averaged across trials (*bottom*; bin size, 20 ms). *Bottom*, population average of instantaneous firing rate before, during, and after yellow-light illumination (*black line*, mean; *gray lines*, mean \pm SE; n=13 units). (d–e) Adapted from (18).

expressed in neurons, can mediate modest inhibitory currents on the order of 40–100 pA in response to yellow-light illumination (12, 13), enabling moderate silencing of neural activity (Fig. 1c). Halorhodopsins have same intrinsic kinetic limitations, with some photocycles taking tens of minutes to complete (e.g., Fig. 4a, b; (12, 14)), and halorhodopsins also require improved trafficking for expression at high levels (15–17). A third class of microbial opsin, the bacteriorhodopsins, is exemplified by the light-driven outward proton pump archaerhodopsin-3 (Arch/aR-3), from the archaeal species Halorubrum sodomense. Arch can mediate strong inhibitory currents of up to 900 pA (Fig. 1d), capable of mediating near-100% silencing of neurons in the awake-behaving mouse or monkey brain in response to yellow-green light (Fig. 1e, (15, 18)). Protons are extremely effective as a charge carrier for mediating neural silencing, and proton pumps have greatly improved kinetics with respect to halorhodopsins (Fig. 4c, d), as well as a fast photocycle and efficient trafficking to membranes. Furthermore, outward proton pumps, perhaps surprisingly, do not alter pH to a greater extent than do other opsins (such as ChR2) or than does normal neural activity. The broad and ecologically diverse class of outward proton pumps, which includes blue-green light-drivable outward proton pumps such as the Leptosphaeria maculans opsin Mac (Fig. 5), enables, alongside the yellow-red-drivable Halo, multi-color silencing of independent populations of neurons (15). Also, because the neural silencers Halo and Arch are activated by yellow or yellow-green light, and the neural depolarizer ChR2 is driven by blue light, expression of both a silencer and a depolarizer in the same cell (either by using two viruses, or by using the 2A linker to combine two opsins into a single open reading frame (12, 19) enables bidirectional control of neural activity in a set of cells. This is useful for testing necessity and sufficiency of a given set of neurons in the same animal, or for disruption of neural synchrony and coordination through "informational lesioning" (19).

In the sections below, we describe the properties of these three opsin classes, as well as genetic (e.g., viral and transgenic) and hardware (e.g., lasers and LEDs) infrastructures for using these opsins to parse out the function of neural circuits in a wide variety of animal nervous systems. A theme of this field is that extremely rapid progress and adoption of these technologies have been driven by technology development curves in other fields such as gene therapy and optical imaging. Our hope is to convey a snapshot of this rapidly moving field as of 2009–2010, summarizing the first half-decade of its existence, to teach both neuroengineers hoping to innovate by inventing new tools, and neuroscientists hoping to utilize these tools to answer new scientific questions. We will first survey the general properties of these opsins (Sect. 2), then go into the channelrhodopsins (Sect. 3), followed by the neural silencing pumps (halorhodopsins and bacteriorhodopsins, Sect. 4), the molecular strategies for delivering these genes to cells for appropriate expression in vitro and in vivo (Sect. 5), and the hardware for illuminating these opsin-expressing neurons in vitro and in vivo (Sect. 6).

2. Properties of "Optogenetic" Microbial (Type I) Opsins

The three classes of molecules described to date are from organisms such as unicellular algae, fungi, and archaea, whose native environments and membrane lipid composition are very different from those of mammalian neurons. Thus, the performance of these molecular tools in neurons can be difficult to predict based solely upon their properties in other species, and must be assessed empirically for assurance of efficacy and safety. Nevertheless, there are several molecular properties that contribute to efficacious, temporally precise optical control of neurons, which can be explored in a unified and logical fashion:

- *Initial protein expression levels*: The efficiency of ribosomal translation of a molecule is largely affected by codon optimization. It is recommended that genes codon-optimized for the target species be used.
- *Membrane insertion properties, protein folding, and interactions with local environment*: Increased membrane localization will result in more functional molecules and thus increased photocurrents. This property may also be inversely associated with the potential property of *toxicity*, since poorly trafficked or folded molecules may aggregate in the cytosol and endoplasmic reticulum. On the contrary, if a molecule has adverse intrinsic side effects, enhanced trafficking may exaggerate them. Furthermore, any given channel or pump will best operate under defined conditions (e.g., chloride conductance, pH, and lipid environment), which may not exist in a given target cell type.
- *Innate conductance and permeability*: Channels translocate more ions per photocycle than pumps, because channels open up a pore in the membrane, unlike pumps. On the other hand, pumps can move ions against concentration gradients. Each opsin furthermore passes a precise set of ions in a specific cellular context, and not others.
- *Photocycle kinetics*: Both light-driven channels and pumps are described by a photocycle, the list of states that a molecule goes through after light exposure, including ion-translocating or ion pore-forming steps. The faster the photocycle, the more temporally precise the molecular function might be, and for a pump, the more ions will be translocated. (For a channel, a faster photocycle may result in the channel entering the ion

pore-forming state more often, but may also reduce the time spent in the open state). If a molecule enters an inactive photocycle state for an enduring period of time, it may be effectively nonfunctional.

- *Photosensitivity*: Molecules may require different amounts of light to begin moving through their photocycle, based on the chromophore absorption efficiency. Furthermore, from an end-user standpoint, effective photosensitivity will appear to be a function of the overall photocycle; for example, a pump that has a slow photocycle may appear to be light insensitive (because incident photons may have no effect on the molecule during the photocycle), whereas a channel that inactivates extremely slowly may appear to be light sensitive (because each photon will result in large charge transfers).
- *Action spectrum*: Different molecules are driven by different colors of light. Multiple cell types can be orthogonally addressed with different colors of light if they express opsins whose action spectra minimally overlap.
- *Ion selectivity*: Unlike traditional electrodes, microbial opsins can generate ion-specific currents, since they will pass specific ions such as chloride (Cl⁻) or calcium (Ca⁺²). This opens up novel kinds of experimental capability, such as the ability to test the sufficiency of a given ion, in a given location, for a given biological function.

We will, in the following sections, frame current knowledge about cell type-specific optical control of neurons, in the context of decades of research in structure-function relationships of microbial (type I, or archaeal) opsins. In many ways, these molecules are similar in tertiary structure to mammalian (type II) rhodopsins (20), the pigments that confer photosensitivity to the rods and cones of the human retina. Both types are composed of seventransmembrane (7-TM) α -helices, linked by six loop segments, and their photosensitivity is enabled by a retinal bound to a specific lysine residue near the C-terminus, forming a Schiff base that undergoes a trans-cis or cis-trans isomerization upon illumination, which then induces conformational changes in the protein. However, they are evolutionarily unrelated, and their differences have important implications for their use in perturbing neuronal activity. Mammalian rhodopsins (21) are very sensitive photon detectors, optimized for sensitivity rather than speed. They utilize 11-cis retinal as the primary chromophore, which isomerizes to all-trans retinal upon absorbing a photon. The resultant structural change activates an associated G-protein, transducin, which then initiates a cascade of secondary messengers. The all-trans retinal dissociates from the opsin, is converted back to its 11-cis form, and then re-associates with the apoprotein to reconstitute a functional molecule – a process that typically takes hundreds of milliseconds, too slow to enable fast control of neurons in the central nervous system. On the contrary, a microbial opsin utilizes all-trans retinal as its chromophore, which isomerizes to 13-cis retinal upon absorbing a photon. The chromophore does not undergo a quasi-irreversible dissociation event, but rather thermally relaxes to its active all-trans form in the dark (although this process can be facilitated by light). The trans-cis isomerization sets off several coupled structural rearrangements within the molecule that accommodate the passive conduction or active pumping of ions (22-24). Ultimately, this means that at the expense of light sensitivity, archaeal opsins can deflect the membrane potential of a cell on the scale of hundreds of microseconds to a few milliseconds. However, it should be noted that genetically targetable, optical neural silencing has also been demonstrated using mammalian G-protein-coupled receptors, which can couple to potassium channels (4), and genetically targetable optical neural activation has been demonstrated using melanopsins and invertebrate-style rhodopsins, at the price of temporal precision (25, 26).

As an exemplar of a well-characterized microbial opsin reagent, with crystal structure and photocycle both well-described, Fig. 2 shows the crystal structure of the light-driven chloride-pump



Fig. 2. Structure and function of halorhodopsin. (a) Crystal structure of halorhodopsin, which is composed of seventransmembrane α -helices (7-TM) and a retinal chromophore that forms a Schiff base to a lysine near the C-terminus (from (27)). (b) Schematic of the halorhodopsin structural rearrangements and their relation to pumping activity at various points in the photocycle. Image modified from (24). (c) The halorhodopsin photocycle at high-power continuous illumination on the timescale of a typical photocycle (i.e., conditions used for neural silencing, >few ms). The HR410 intermediate is the origin of the long-lived inactivation in neural silencing (e.g., (12, 14)).

halorhodopsin (Fig. 2a; (27)), as well as schematized structural rearrangements that are hypothesized to occur as the molecule pumps a chloride ion across the membrane and into the cytoplasm (Fig. 2b; (24)). While it is convenient to consider the molecular tools discussed here as toggle switches for turning neurons on and off, it is critical for use of these opsins to realize that the translocation of ions by microbial opsins is not as simple as that in a two-state toggle switch. The structural rearrangements constitute an active advancement through a complex photocycle with various intermediate states beyond the initial phototransition (Fig. 2c). There exists a very rich literature on type I microbial opsins from an evolutionary and protein structure-function perspective. The canonical molecules include the proton-pumping bacteriorhodopsin (BR), the chloride-pumping halorhodopsin (HR/sHR/HsHR) from Halobacterium salinarum (halobium), and the halorhodopsin from N. pharaonis (Halo/NpHR/pHR). These were some of the first membrane proteins crystallized, and a myriad of structure-function studies have been performed on these molecules (11, 14, 20, 22-24, 27-45). These studies will not be reviewed here, but it is important to point out their existence because much of what we know with respect to the photocycle and structure of opsins comes from these studies and from sequence homology of novel opsins to these canonical molecules. As will be shown later, for example, a deep understanding of the literature has enabled some researchers to derive powerful new variants of channelrhodopsin (5, 6, 8, 10), even though no crystal structure exists for this molecule.

3. Optical Neural Stimulation: Channelrhodopsins

Channelrhodopsins are the primary photoreceptors in the eyespot of the unicellular algae that are responsible for phototactic and photophobic responses (46-48). Their name is derived from the fact that despite the sensory function, the 7-TM segment is in itself a light-activated ion channel. While the channel pore and properties remain poorly understood, it has been realized recently that channelrhodopsins are likely proton pumps like many other microbial opsins, but with a leaky step in the photocycle during which the opsin lets positive charge into cells (49). In C. reinhardtii, two separate channelrhodopsins were originally identified (48), one with fast kinetics but poor light sensitivity, channelrhodopsin-1 (ChR1) (50), and another with slower kinetics but improved sensitivity, channelrhodopsin-2 (ChR2) (1). Two more channelrhodopsins from V. carteri (VChR1 and VChR2) have also been identified (7, 51), and as will later be discussed, many more ChRs are expected to exist. ChR1-style channelrhodopsins have

red-shifted action spectra (peak $\lambda_{ChR1} = 500 \text{ nm}$, $\lambda_{VChR1} = 535 \text{ nm}$) relative to ChR2 (peak $\lambda_{ChR2} = 470 \text{ nm}$), and thus in principle, ChR1-style and ChR2-style opsins could be used together to drive separate sets of neurons with two different colors of light, if suitably spectrally separated opsin pairs could be found.

Channelrhodopsins (abbreviated as ChRs, chops) are light-activated, inwardly rectifying cation channels that are, at neutral pH, permeable to physiologically relevant cations such as H⁺, Na⁺, K⁺, and Ca²⁺, with permeabilities (relative to sodium) of 1×10^6 , 1, 0.5, and 0.1, respectively (1, 6, 46, 50). It is of particular note that the proton conductance (G_{H+}) is 10⁶-fold larger than the sodium conductance (G_{Na+}), and thus it is expected that at near physiological pH, perhaps half the photocurrent is carried by protons (46); therefore, ChRs may rapidly equilibrate the intracellular pH with its environment (10). Kinetic selectivity analysis has shown that the mechanism of ion selectivity is likely to be due to differential binding affinity of channelrhodopsin channel residues for different ions, not differential ion transport rates (46).

ChR1 was originally believed to be a selective proton channel (50); however, it was later discovered that the poor photocurrents at mammalian pH were likely attributable to poor membrane localization (6), and the apparent lack of sodium currents in the original report was due to the low pH used to perform experiments in that study; the sodium conductance of ChR1 lessens at low pH (6, 46), unlike that of ChR2 (6). This highlights what will be a recurrent theme throughout this chapter: effective conductance in a heterologous system is determined not only by the innate kinetic and transport properties of the molecule, but also by its trafficking and performance in the environment of the heterologous system.

The single ion channel conductance of ChR2 has been estimated at 50 fS (1), which corresponds to approximately 3×10^4 ions per second, or 300 ions per photocycle event, assuming a 10-ms turnover. This is considerably less than that of a typical voltage-dependent sodium channel that may have a conductance on the order of ~10 pS. It has been estimated from electrophysiological data that 10^5 – 10^6 membrane-embedded ChR2 molecules are required to cause reliable spiking in cultured rodent hippocampal neurons (52), with saturation of blue-light densities of several mW/mm² both in vitro (10) and in vivo (53).

Figure 3a shows a typical photocurrent trace from a voltageclamped neuron expressing ChR2 (top), and the spiking pattern that would result in current-clamp mode (bottom). There is a large transient peak with an opening time constant near 1 ms (1, 6, 10), although photocurrent onset can be measured at <200 µs (1, 3,54); this transient peak quickly decays to a stationary component

3.1. Conductance, Permeability, and Context

3.2. Basic View of Kinetics and Wavelength Selectivity



Fig. 3. Channelrhodopsin kinetic and photocycle properties, and impact on neural activity. (a) ChR2 currents elicited in a voltage-clamped hippocampal neuron expressing ChR2 and illuminated by blue light (*top*), and ChR2-driven spikes elicited in a current-clamped hippocampal neuron (three repetitions of the same blue-light pulse in the same neuron) (*bot-tom*), under 1 s of blue-light illumination. Adapted from (3). (b) The photocycle of ChR2 determined by a combination of spectroscopy, site-directed mutagenesis, and electrophysiology, adapted from (49). The *inner circle* summarizes the effective appearance of the photocycle, an approximation to the outer photocycle. (c) The interplay between photocycle, wavelength, and electrophysiological activity. ChR2 is excited with blue light for a brief period, and then a green light is turned on. The photocurrent initially diminishes because the channel is forced to close, but then increases because the green light also pumps the molecule into its most highly efficient state. Image modified from (54).

that is typically <20–50% of the initial peak photocurrent (1, 3, 6, 10). Upon removing the light, ChR2 closes with a time constant of 10–20 ms (1, 6, 10). The transient photocurrent peak is highly dependent on the illumination intensity (51, 55) and history (1, 3, 10); the history dependence results from a desensitization of the transient component that takes ~5 s to recover from in the dark (3). The stationary component on the contrary is less photosensitive and effectively history independent (55). ChR2 absorbs maximally at 460 nm (1, 10), and the action spectra of both temporal components are nearly identical in ChR2.

The large and fast-onset peak enables ChR2-expressing neurons to spike with exquisite temporal precision on the millisecond timescale (Fig. 1b), the timescale of an action potential. However, the large inactivation (or alternatively, the small stationary component) and its slow recovery in the dark, as well as the slow closing rate of ~10–15 ms, ultimately limit the ability to drive reliable spike rates >25 Hz (3, 10) because (1) the stationary photocurrent may be too small to depolarize a neuron to spike threshold sufficiently and (2) the channel cannot physically close quickly enough to enable de-inactivation of sodium channels. It should be noted, though, that many neurons, such as pyramidal cells, seldom fire action potentials at this rate on the individual neuron level (vs. population synchrony or rhythmogenesis).

ChR1-style channelrhodopsins (VChR1 and ChR1) (7, 50) on the contrary demonstrate dramatically faster kinetics than ChR2-style channelrhodopsins (VChR2 and ChR2). The stationary photocurrents of ChR1s are >70% of the peak photocurrents, and the channels open and close approximately two- to threefold faster than does ChR2. Therefore, one would expect that given comparable expression, protein folding, membrane localization, and photosensitivity (i.e., factors contributing to effective conductance), ChR1s would be capable of driving spike rates with greater fidelity than ChR2s. However, poor membrane expression limits the performance of natural ChR1-style channelrhodopsins (7, 50). Chimeras composed of the first five helices of ChR1 and last two helices of ChR2 have been constructed (6, 10, 56), and these new variants exhibit the small inactivation and action spectrum of ChR1, but the overall effective conductance of ChR2. These structure-function studies will be discussed in detail later in this chapter. A point mutant of this chimera dubbed "ChIEF" (based on its composition as a [Ch]annelrhodopsin chimera with an [I]190V substitution with domains swapped between ChR1 helix-[E] and ChR2 helix-[F]), developed by Tsien and coworkers (10), appears to be a highly improved tool for stimulating neurons. Its large stationary photocurrent and very fast channel closing, the latter conferred by the I190V mutation, contribute to far more reliable spiking (up to 100 Hz) than that of ChR2.

Based on the available characterization of the channelrhodopsins from *V. carteri* (7, 51), the general characteristics are similar to those of the analogous molecules in *C. reinhardtii*. VChR2 and ChR2 have nearly identical photocycles and action spectrum (51). VChR1 and ChR1 exhibit similar reduced inactivation, and are both red-shifted from their respective VChR2/ChR2 counterparts. It has been proposed that VChR1 could be used for multicolor optical stimulation in conjunction with ChR2, which is blue-shifted by ~70 nm, but further improvements are likely required for reliable spiking because the VChR1 photocurrents are unfortunately approximately four- to fivefold smaller (7), and also there is significant spectral overlap between VChR1 and ChR2.

3.3. Detailed Models of Kinetics and Wavelength Selectivity

s As previously mentioned, it is critical to realize that the translocation of ions by opsins is not as simple as the operation of an on/off switch, but rather these opsins traverse a complex photocycle with various intermediate states beyond the initial opening of the channel.

Figure 3b shows the photocycle of ChRs based on photophysical studies performed primarily by laser flash spectroscopy, physiology, and site-directed mutagenesis (8, 49, 51, 54, 57). Importantly, the intermediates of the photocycles themselves can also undergo photoreactions, and thus they may be optically driven or "short circuited" (54) between photointermediates at much faster rates (Fig. 3c). The ChR2 photocycle begins in its closed dark-adapted state D470 (where the number in the state name corresponds to the peak light absorption, in nanometer, of the molecule in that state). The channel opens when D470 absorbs a photon, after which the molecule will become a green absorbing photoproduct or P-intermediate, P520, via thermal relaxation from short-lived photoproducts. This initial cascade of events takes 0.2-1.5 ms, depending on the transmembrane potential. The open ChR2 can be closed by either optically pumping P520 \rightarrow D470 with green light, or by decaying to P480 (via a yet-to-be-determined intermediate), a process that takes ~6 s. The inactivation toward the stationary photocurrent may be due to molecules making the P520->P480 transition, rather than the optically induced P520 \rightarrow D470 transition that would allow the molecule to open again quickly. Assuming that ChR1 and ChR2 photocycles are topologically similar, e.g., the ChR2 D470 and P480 equate to the ChR1 peaks at 464 and 505 nm, this interpretation of the transient and stationary photocurrents is consistent with the finding that for ChR1, the stationary photocurrent is red-shifted from the transient photocurrent (6).

The various wavelengths of absorption of rhodopsins and their intermediates throughout the photocycle arise from the different conformations of the chromophore and its local environment, which influences the chromophore charge distribution and the protonation of the retinylidene Schiff base. Figure 3c demonstrates this complex interplay in an experiment by Bamberg and coworkers (54). After blue-light-excited ChR2 has reached its steady state, a green-light costimulation is introduced. The photocurrent briefly diminishes because the open channel is forced to close, but the stationary photocurrent quickly improves because many molecules have been pumped back into their highly efficient, peak-producing state. Thus, it is possible that slightly redshifted or broadband illumination of ChR2 may strike a balance between optimally exciting the dark state (transient component) and repriming the dark state (driving the red-shifted intermediate photoproduct). As will be discussed, optimal silencing with N. pharanois halorhodopsin is analogously achieved by using both yellow light to hyperpolarize the neuron and blue light to drive the molecule out of its inactive state (12, 14).

3.4. MutantsAs previously mentioned, even though no ChR crystal structure
exists at the time of this writing, useful structure–function studies
have been performed based largely on sequence homology to
H. salinarum bacteriorhodopsin. The E90Q mutation (57) has

increased sodium selectivity (with respect to G_{H_+}) vs. wild-type ChR2, and the H134R mutant (5) demonstrates increased conductance by approximately twofold. Various mutations to C128 (8) corresponding to bacteriorhodopsin T90 drastically slow down the rate of ChR2 closure from the open state, thus effectively creating a bistable open P520 state until illuminated with green light. By lengthening the time that ChR2 spends open on a per-photon basis, this mutation effectively decreases the amount of light needed to activate the channel, at the expense of temporal precision.

Chimeras of ChR1 and ChR2 have been constructed by several researchers (6, 10, 56), one of which was that composed of ChR1 helices A–E and ChR2 helices F–G (called abcdeFG, ChEF, or ChR1/2_{5/2} by various investigators). These chimeras displayed the small inactivation of ChR1, but the large photocurrents of ChR2 on account of improved membrane localization and light sensitivity (based on quantitative confocal fluorescence microscopy, (6)). An I190V substitution to ChEF led to the molecule "ChIEF" that is capable of driving more reliable fast spiking due to the much larger stationary current and faster channel closing kinetics after light offset (10). During these studies, it was also discovered that a single point mutation to wild-type ChR1, E87Q, eradicates its pH-dependent spectral shifts and increases inactivation during illumination (56).

The fact that the poor effective conductance of ChR1 can be largely attributed to membrane localization rather than its photophysical properties highlights the importance of considering and improving the trafficking of heterologously expressed molecules. In particular, ChRs are not localized to the outer membrane but rather the eyespot in *C. reinhardtii*, and the membrane composition of the organism is less than 20% phosphoglyceride (58), a primary lipid type in mammalian neurons. As will be discussed later, in the context of halorhodopsins, the use of signaling peptides can improve outer membrane localization and reduce aggregation in the cytosol, endoplasmic reticulum, and Golgi apparatus.

Along similar lines of using signal peptides to alter trafficking, the myosin-binding domain (MBD) peptide promotes subcellular localization of opsins to neuronal dendrites (9). This subcellular localization strategy may prove to be helpful for enabling driving of electrical activity in specific neural compartments, or for high-resolution connectomic mapping in vivo. Two-photon excitation is a powerful laser excitation technique that enables submicron resolution in 3D (59) relatively deep in the brain (~750 μ m, or a significant fraction of the thickness of the mouse cortex), but its ability to induce action potentials in a neuron expressing ChR2 is limited by the interplay between molecule density and the extent of optical depolarization with respect to time (60, 61). The probability of inducing an action potential, at low powers that are not destructive to tissue, is relatively low using a traditional raster scan because the fraction of molecules excited at any point in time is small, and most photons that do hit the membrane are wasted (since the open time of ChR2 is long relative to a femtosecond laser photon delivery rate). Thus, with most conventional two-photon laser scanning methods, the aggregate contributions of the serially excited molecules never sufficiently depolarize the whole neuron to spike threshold. However, Rickgauer and Tank have demonstrated that neurons expressing ChR2 can be reliably excited by two-photon microscopy by optimizing the scan pattern to deliver light optimally to the cell membrane, in a fashion that reaches the maximum surface area while minimizing wastage of photons on already-lightdriven channelrhodopsin molecules (61).

3.5. Diversity Unlike microbial rhodopsins from archaea, significantly less is known about the photo-electrogenic molecules of unicellular algae, the only organisms known to date to have naturally occurring light-activated channels. Photoelectric responses have been measured in several green flagellates, as well as in phylogenetically distant cryptophytes (47, 62–64). Interestingly, the two-component phototaxis strategy employed by *C. reinhardtii*, in which the response is mediated by a fast (ChR1) and slow (ChR2) rhodopsin, appears to be general (47), which begs the question whether chimeras of their respective rhodopsins will also result in kinetic improvements and variants with interesting properties. Thus, as more phototaxis-mediating rhodopsins are isolated and sequenced, new molecular tools for controlling neurons will surely emerge.

4. Optical Neural Silencing: Halorhodopsins and Bacteriorhodopsins

Whereas traditional electrodes can stimulate neurons with temporal precision (albeit without cell type specificity), they are incapable of silencing neurons in order to assess their necessity for given neural computations, behaviors, and pathologies. Therefore, there is a large need for spatio-temporally precise methods for optical inhibition of neurons. Inwardly rectifying chloride pumps and outwardly rectifying proton pumps, halorhodopsins (HRs, hops) and bacteriorhodopsins (BRs, bops), respectively, are electrogenic pumps that when heterologously expressed are capable of sufficiently hyperpolarizing a neuron to silence its activity (Fig. 1c–e; (12, 15, 65)). They are thus far known to exist in every kingdom except in animals: archaea (22, 23, 66–68), bacteria (69–75), fungi (76, 77), and algae (78). In addition to their opposite electrophysiological effect, HRs and BRs differ primarily from channelrhodopsins in that their physiological functions are chiefly due to their role as pumps as opposed to operating as passive channels, and thus can translocate ions against concentration gradients (but typically only one ion per photocycle). Much is known about the photocycles and structure–function relationships of HRs and BRs because they have been crystallized (24, 27, 28, 79, 80) and heavily characterized via spectroscopy, mutagenesis, and physiology for decades.

This section will focus on two molecules in particular: *N. pharaonis* halorhodopsin (Halo/NpHR) and *H. sodomense* bacteriorhodopsin (Arch/AR-3), also known as an archaerhodopsin (i.e., a bacteriorhodopsin from the *Halorubrum* genus). Halorhodopsins were shown in 2007 to be capable of mediating modest optical neural hyperpolarizations, and since then have been improved in trafficking to boost their currents (12, 13, 16); bacteriorhodopsins were shown in 2009 to be able to mediate very powerful and kinetically versatile silencing of multiple neural populations with different colors of light (18). We will discuss in the following section "Conductance, permeability, and context" and "Kinetics and wavelength selectivity" of halorhodopsins and bacteriorhodopsins for these two classes separately, followed by a joint discussion of the "Mutants and variants" and genomic "Diversity" in a unified section.

4.1. Halorhodopsins: Conductance, Permeability, and Context

N. pharanois halorhodopsin (NpHR, Halo) is a highly selective, inwardly rectifying chloride pump, which can also conduct larger monovalent anions (81). It has a reversal potential of approximately -400 mV (81), and its chloride dependence of pumping activity (full- and half-saturating chloride concentrations: $[Cl^{-}]_{saturation} = 20 \text{ mM}, [Cl^{-}]_{1/2} = 2.5 \text{ mM}) (82)$ is appropriate for operation in mammalian cells, whereas H. salinarum halorhodopsin is not capable of effective operation in mammalian neurons (15), presumably because of its large chloride dependency: $[Cl^{-}]_{saturation} = 5 \text{ M and } [Cl^{-}]_{1/2} = 200 \text{ mM} (82, 83).$ In the absence of any signal peptide sequences to improve trafficking and membrane localization, Halo has been reported to generate 40–100 pA of hyperpolarizing current (12, 18, 65), with the differences in measured photocurrents between studies largely attributable to the power and wavelength of excitation used. This photocurrent is approximately 10- to 25-fold less than typical peak depolarizing currents generated by ChR2, highlighting one potential disadvantage inherent to a pump that translocates one ion per photocycle (e.g., Halo) vs. a channel that conducts 300 ions per photocycle (e.g., ChR2). To mediate these currents, there are an estimated ten million membrane-embedded Halo molecules per neuron (as assessed in hippocampal neuron culture). Because the expression levels are so high, Halo is known to form puncta or intracellular blebs, aggregating in the endoplasmic reticulum (ER) and Golgi apparatus (16, 17). These issues are somewhat

addressed by attaching trafficking enhancement sequences to the molecule, e.g., a C-terminal ER-export sequence from the KiR2.1 protein (eNpHR), which increases the effective conductance by about 70% by increasing membrane expression (16).

Recently, we discovered that the crux-halorhodopsin (HR from the Haloarcula genus) from Haloarcula marismortui, canonically known as cHR-5 (68, 84), produces photocurrents similar to Halo with more uniform expression; even when highly overexpressed under high copy number transfection conditions, no puncta or intracellular blebbing is observed (15). This molecule may better express than Halo in vivo, but it remains unknown at this moment whether it will ultimately be more efficacious at altering mammalian behavior, given their statistically insignificant difference in photocurrent. However, the prolactin (Prl) ER-location sequence in conjunction with a signal sequence from an MHC class I antigen triples the Halo photocurrent (15, 18); we are now trying out multiple trafficking sequences in combination to see if they boost current further. However, it is important to note that if halorhodopsins have other side effects that are due to the protein's intrinsic properties - for example, one paper quantitates the significantly altered neuronal capacitance that results from expressing halorhodopsin in neurons in vivo (85) – then boosting expression may only make such side effects worse.

4.2. Halorhodopsins: Kinetics and Wavelength Selectivity

N. pharaonis halorhodopsin is capable of silencing weakly firing neurons on the millisecond timescale with its ~100 pA scale currents, with rapid onset and offset (12), but during long periods of illumination, all halorhodopsins that we have tested so far and that have current (from Natronomas pharaonis, Halorubrum sodomense, Haloarcula vallismortis, Haloarcula marismortui, and Salinibacter ruber) inactivate by approximately 30% every 15 s of illumination at 1–10 mW/mm² of yellow (593 nm) light (Fig. 4a, b; (12, 18)). This slow inactivation stands in contrast to that in ChR2, which responds to light with a large transient peak that decays within seconds, followed by a stable stationary photocurrent. For all of the halorhodopsins named above, recovery in the dark from light-induced inactivation is slow, with a time constant of tens of minutes, as has been described for some halorhodopsins earlier (12, 14, 39) (Fig. 4a, b). This long-lasting inactivation property may hinder the use of halorhodopsins for silencing for prolonged periods, e.g., during repeated behavioral trials. Importantly, for all halorhodopsins investigated, the inactive photoproduct can be driven back to its active pumping state with a short (e.g., subsecond duration) pulse of blue or UV light (12, 14); thus, optimal use of Halo for neural silencing requires both yellow and blue light to be delivered to the same set of neurons, which is possible (86) but can complicate optics setups.



Fig. 4. Kinetic Comparisons between halorhodopsins and archaerhodopsins. (a) (i) Timecourse of Halo-mediated hyperpolarizations in a representative current-clamped hippocampal neuron during 15 s of continuous yellow light, followed by four 1-s test pulses of yellow light (one every 30 s, starting 10 s after the end of the first 15-s period of yellow light). (ii) Timecourse of Halo-mediated hyperpolarization for the same cell exhibited in (i), but when Halo function is facilitated by a 400-ms pulse of blue light in between the 15-s period of yellow light and the first 1-s test pulse. (b) Population data for blue-light facilitation of Halo recovery (n=8 neurons). Plotted are the hyperpolarizations elicited by the four 1-s test pulses of yellow light, normalized to the peak hyperpolarization induced by the original 15-s yellow-light pulse. *Dots* represent mean \pm SEM. *Black dots* represent experiments when no blue-light pulse was delivered (as in Fig. 6.5ai). *Open blue dots* represent experiments when 400 ms of blue light was delivered to facilitate recovery (as in Fig. 6.5aii). (c) Raw current trace of a neuron lentivirally infected with Arch, illuminated by a 15-s light pulse (575 \pm 25 nm, irradiance 7.8 mW/ mm²), followed by 1-s test pulses delivered starting 15, 45, 75, 105, and 135 s after the end of the 15-s light pulse. (d) Population data of averaged Arch photocurrents (n=11 neurons) sampled at the times indicated by the *vertical dotted lines* that extend into Fig. 4c.

The Halo photocycle is shown in schematic form in Fig. 2c. The time constants listed are the limiting ones, with all other transitions <100 μ s. It should be noted that the names for canonical spectroscopic states of *H. salinarum* halorhodopsin – the K, L, N, and O photointermediates – have not been used here because the order of the N and O states in *N. pharaonis* halorhodopsin is still somewhat debated (42, 87, 88). In the dominant photocycle, Halo absorbs a photon and then within tens of microseconds, quickly releases a chloride ion into the cytoplasm during the HR520 \rightarrow H640 transition, via short-lived intermediates that "switch" the chloride location within the molecule from the extracellular loading domain to the cytoplasmic release domain. The molecule then re-isomerizes from the HR640 state and takes up a chloride ion from the extracellular side, a process that takes ~1.5 ms; it then forms the HR' state, which finally relaxes to the active ground state with a time constant of ~20 ms. However, halorhodopsins can enter an alternate photocycle (middle trajectory within Fig. 2c), most notably under prolonged or bright illumination, as might occur during in vivo neural silencing. The 13-cis retinylidene Schiff base becomes deprotonated (releasing a proton into the cytoplasm and thus introducing a small depolarizing proton current) and forms a long-lived intermediate HR410 (14, 39). In the dark, the halorhodopsin will remain in this inactive state for a duration on the order of $30 \min(39)$. This formation of HR410 is the origin of the long inactivation observed in neurons expressing halorhodopsin and the ability to recover the active state using the short blue light pulse (12, 14). In contrast, as will be discussed in detail in the next section, archaerhodopsins (bacteriorhodopsins from the Halorubrum genus) spontaneously recover in the dark under physiological conditions.

4.3. Bacteriorhodopsins: Conductance, Permeability, and Context Arch, canonically known as archaerhodopsin-3 (AR-3) from *H. sodomense*, is a yellow-green light-sensitive, outwardly rectifying proton pump with nearly an order of magnitude increase in hyperpolarizing current over any characterized natural halorhodopsin (15, 18), attaining neuronal currents up to 900 pA in response to light powers easily achievable in vitro or in vivo. The efficacy of these proton pumps is surprising, given that protons occur, in mammalian tissue, at a millionfold lower concentration than the ions carried by the optical control molecules described above. This high efficacy may not only be due to the fast photocycle of Arch (see also (89, 90)), but may also be due to the ability of high-p K_a residues in proton pumps to mediate proton uptake (89, 91).

Arch is a highly efficacious tool in vivo, with cortical neurons in the awake-behaving mouse undergoing a median of 97.1% reductions in firing rate for periods of seconds to minutes (Fig. 1e) (18), and safely expresses for months in both mice and monkeys when virally delivered in vivo. Due to the larger currents, Arch enables very large (e.g., order of magnitude scale) increases in addressable volume of silenceable tissue, over earlier reagents. We thoroughly investigated the safety of Arch function. To date, blebbing issues that have affected the usage of halorhodopsins have not been observed in vitro or in vivo for Arch, but membrane trafficking sequences may still prove effective at boosting expression beyond the natural state (the Prl sequence, which greatly magnifies Halo current, slightly increases Arch current in neurons). Furthermore, we have not observed changes in cell membrane capacitance or other passive neural properties, as has been reported with halorhodopsin expression (see above). From an end-user standpoint, illumination of Arch neurons was safe: spike rates measured in vivo were not significantly different before

vs. after periods of optical neural silencing. Biophysically, pH changes in neurons expressing Arch and undergoing illumination were minimal, plateauing rapidly at alkalinizations of 0.1-0.15 pH units; the fast stabilization of pH₁ may reflect a self-limiting influence that rapidly limits proton concentration swings, and may contribute to the safe operation of Arch in neurons, as observed in mice and monkeys. Indeed, the changes in pH observed in cells expressing Arch and being illuminated are comparable in magnitude to those observed during illumination of ChR2-expressing cells (10) (due to the proton currents carried by ChR2 (1, 46)) and are also within the magnitudes of changes observed during normal neural activity (92-95). We have observed that other archaerhodopsins from other Halorubrum strains are also particularly powerful molecular reagents (work in progress). In contrast, the canonical H. salinarum bacteriorhodopsin, well known to function poorly in E. coli, successfully produced modest photocurrents in mammalian neurons, which highlights the importance of not assuming that all molecules will express and traffic in the same manner in different organisms. (In contrast, E. coli does not support any detectable expression of ChR2, which expresses well in neurons; target species' influences in modulation of opsin function should not be underestimated).

4.4. Bacteriorhodopsins: Kinetics and Wavelength Selectivity Unlike all of the halorhodopsins we have screened to date (including not only the natural halorhodopsins described above, but also products of halorhodopsin site-directed mutagenesis aimed at improving kinetics), which after illumination remained inactivated for tens of minutes, Arch spontaneously recovers its function in seconds in the dark (Fig. 4c, d), more like the light-gated cation channel channelrhodopsin-2 (ChR2) than like halorhodopsins. This feature is particularly useful for in vivo behavior work because it dramatically simplifies the necessary optical hardware; the need to use only one wavelength of light also increases the available bandwidth for multicolor silencing in multiple cell types. We have also observed this spontaneous recovery with other archaerhodopsins, and thus it may be a general feature of archaerhodopsins as a whole (work in progress).

Arch is maximally excited with green-yellow light ($\lambda = 561 \text{ nm}$), a fairly common peak wavelength for proton pumps. Thus it is backwards compatible with halorhodopsin-driving equipment. Proton pumps naturally exist that are activated by many colors of light, in contrast to chloride pumps, which are primarily driven by yelloworange light (even with significant mutagenesis of retinal-flanking residues, (15)). The light-driven proton pump from *L. maculans*, abbreviated Mac, has a strongly blue-shifted action spectrum relative to that of the light-driven chloride pump Halo (Fig. 5a). We found that Mac-expressing neurons could undergo 4.1-fold larger hyperpolarizations with blue light than with red light,



Fig. 5. Multicolor silencing of two neural populations, enabled by blue- and red-light drivable ion pumps of different classes. (a) Action spectra of Mac vs. Halo; *rectangles* indicate filter bandwidths used for multi-color silencing in vitro. Blue-light power is via a 470 ± 20 nm filter at 5.3 mW/mm², and red-light power is via a 630 ± 15 nm filter at 2.1 mW/mm². (b) Membrane hyperpolarizations elicited by blue vs. red light, in cells expressing Halo or Mac (n=5 Mac-expressing neurons, n=6 Halo-expressing neurons). (c) Action potentials evoked by current injection into patch-clamped cultured neurons transfected with Halo (i) were selectively silenced by the red light but not by the blue light, and vice versa in neurons expressing Mac (ii). *Gray boxes* in *inset* (iii) indicate periods of patch clamp current injection.

and Halo-expressing neurons could undergo 3.3-fold larger hyperpolarizations with red light than with blue light, when illuminated with appropriate powers and filters (Fig. 5b). Accordingly, we could demonstrate selective silencing of spike firing in Mac-expressing neurons in response to blue light, and selective silencing of spike firing in Halo-expressing neurons in response to red light (Fig. 5c). Thus, the spectral diversity of proton pumps points the way towards independent multicolor silencing of separate neural populations. This result opens up novel kinds of experiment, in which, for example, two neuron classes, or two sets of neural projections from a single site, can be independently silenced during a behavioral task.

Figure 6 shows the photocycle of the canonical *H. salinarum* bacteriorhodopsin, as representative of the photocycle of the class of proton pumps (the photocycles of archaerhodopsins are not as well characterized and may well be different) (22, 91). The data that have led to the synthesis of the modern model of the bacteriorhodopsin photocycle provide many of the insights that have led to solid investigations into this field as a whole. As in Figs. 2c and 3b, it has been simplified to represent the dominant photocycle expected at large and continuous illumination on the timescale of a typical photocycle (e.g., many milliseconds, as



Fig. 6. The photocycle of the *H. salinarum* bacteriorhodopsin. As in Figs. 2c and 3b, the photocycle has been simplified to reflect the dominant photocycle at large continuous illumination on the timescale of a typical photocycle (i.e., conditions used for neural silencing, >few ms). The M412 alternate intermediate is the origin of long-lived inactivation with bacteriorhodopsin. In contrast, Arch spontaneously quickly recovers from this state in the dark.

would be used for neural silencing). Upon absorbing a photon, bacteriorhodopsin forms its L550 intermediate (L=lumi) within microseconds, after quickly transferring a proton from the retinylidene Schiff base (at the Lys-216 position) to the Asp-85 proton acceptor. This transfer triggers the proton releasing group (PRG), containing Glu-204 and Glu-194, to release its own proton (96, 97), during the L \rightarrow M transition. After a "switching" step during which the Schiff base reorients itself on the cytoplasmic side, it is then reprotonated during the $M \rightarrow N$ transition via the Asp-96 donor residue, which in turn picks up a proton from the cytoplasm in the next transition $(N \rightarrow O)$. The chromophore re-isomerizes to the all-trans state during this transition as well. Finally, the bacteriorhodopsin relaxes back to its ground state as the proton release group is reloaded from the Asp-85 residue. Like halorhodopsin, bacteriorhodopsin can become trapped in a long-lasting light-unresponsive state (Fig. 6, "M412 alternate") that requires blue light to re-enter the normal photocycle; this could partly explain the lower currents observed with BR when compared to that in Arch.

4.5. Halorhodopsins and Bacteriorhodopsins: Mutants and Variants

For decades, researchers have been making mutants of bacteriorhodopsins and halorhodopsins for structure-function studies reviewed in many earlier publications (e.g., (22, 24, 91)). However, point mutations that improve these molecules as neural silencing tools have yet to be reported. Given that the conductance of a pump is limited by the fact that they move only one ion per photocycle, it would be highly desirable to mutate halorhodopsin into a channel, or channelrhodopsin into an anion channel. Tuning the action spectrum of both bacteriorhodopsins and halorhodopsins may be achieved by mutating the retinal-flanking residues (74, 75, 98, 99). Mutations that alter ion selectivity, such as the bacteriorhodopsin D85T mutation that converts bacteriorhodopsin into a chloride pump (100), could allow ion-specific currents to be mimicked. A Ca²⁺ selective pump, for example, would have powerful impact on enabling powerful studies of plasticity, synaptic transmission, and cellular signaling. Given that crystal structures for many bacteriorhodopsins and halorhodopsins exist, we anticipate that function-oriented and applied sitedirected mutagenesis will be a highly active field of research in neuroengineering. The fact that archaerhodopsins on the whole represent a class of molecules that express particularly well in mammalian cells possibly indicates properties of their lipid-interacting residues, or perhaps "signal sequence"-like activity by their loop regions. The known crystal structures of these molecules (79, 80) may provide key insights into the trafficking of heterologously expressed molecules and their membrane insertion.

4.6. Diversity Light-activated proton and chloride pumps are known to exist in far more organisms than do light-gated cation channels, and proton pumps are particularly prevalent, as all opsins described to date likely have at least some proton pumping capability (22, 23, 66–78, 101, 102). Even though many proton pumps maximally absorb blue-green to green wavelengths (which opens up, as shown in Fig. 5, the possibility, alongside yellow light-driven chloride pumps, for multicolor silencing of distinct neural populations), light-activated hyperpolarizing currents carried by protons have been observed across the whole visible spectrum, from deep blue (via a sensitizer) (103) to far red (104) (>650 nm), although the red light-sensitive current likely originates from a receptor that triggers an H⁺-ATPase, as opposed to direct light-mediated ion translocation.

The discovery or creation of a purely genetically encoded light-activated inhibitory channel would be highly desirable. In addition to seeking natural molecules and creating site-directed mutants, linking a non-light-gated ion channel to a type I archaeal rhodopsin may be another promising approach to creating such a molecular tool (105). In this way, a light-activated shunt could be created that would more closely mimic natural mechanisms of neural inhibition in the brain.

5. Molecular Targeting of Microbial Opsins to Different Cell Types

The number of papers on optical neural control in species ranging from C. elegans to mouse to nonhuman primate is increasing exponentially each year, and so we will not attempt to review the literature comprehensively. In each species, opsins have been used to test the necessity and sufficiency of neurons, cell types, muscles, neural pathways, brain regions, and other entities in behaviors, pathologies, and neural computations. Opsins have proven valuable in exploring neural dynamics in multiple mammalian brain structures as well. We will focus on highlighting principles that govern how to best use these opsins in various settings, from a molecular biology standpoint (this section, Sect. 5) and from a physical-optical standpoint (next section, Sect. 6). From a molecular biology standpoint, these opsins can be delivered to neurons in almost any conventional way that genes are delivered into cells or into organisms. Transgenic mice have been made with ChR2, for example (106); mice and monkeys have been injected with lentiviruses, adeno-associated viruses (AAV), and other viruses encoding for light-gated proteins (2, 52, 107–109); and rodents and chicks have been electroporated in utero with plasmids encoding for light-gated proteins (4, 53, 110). In each case, different parameters of the technique can be selected so as to enable specific cell types, pathways, or regions to be labeled selectively or to express the opsin selectively. Transgenic *C. elegans* expressing ChR2 have been made using conventional methods (5), as have transgenic Drosophila (111) and zebrafish (112). For these latter species, supplementation with all-*trans* retinal may be beneficial, whereas mammalian brains seem to operate microbial opsins without the need for supplementation. (It is possible that in the future, genetically engineering retinal-lacking organisms, such as invertebrates, to produce retinal within their nervous systems may be of use, for example, by expressing within them enzymes that can produce retinal from vitamin precursors (113)).

For mammalian nervous systems, a large variety of possible strategies exists for conveying opsin genes into specific cell types. For example, transgenic mice can be made through BAC transgenic, knock-in, or other methods, but such strategies are not common for other species yet. For viral delivery, cell type-specific promoters can be inserted upstream of the opsin to target various excitatory, inhibitory, and modulatory neurons (e.g., (19, 114-117)); the size of the promoter is limited by the virus type (AAV viruses hold typically 4-4.5 kb total, whereas lentiviruses hold typically 8–10 kb maximum). The surface or coat proteins that a virus bears can also modulate which cell types will take up the virus; for example, lentiviruses may favor excitatory neurons of the cortex, whereas certain AAV serotypes may favor inhibitory cells (118). Lentiviruses can be pseudotyped – fabricated with a coat protein of desired targeting capacity, e.g., with rabies glycoprotein that leads to lentivirus that travels retrogradely (119) – whereas AAVs can be engineered with biotinylation sites that enable, upon streptavidin conjugation, targeting of potentially arbitrary substrates (120). Retroviruses, which preferentially label dividing cells, have been used to deliver ChR2 to newborn neurons of the dentate gyrus of the hippocampus (121). Other viruses such as rabies virus and pseudorabies virus can be used, with unique tracing capabilities including the ability to go retrogradely across multiple synapses (122, 123). Viral particles typically have to be injected directly into the brain, often through stereotactic targeting to a specific brain area, since the potent blood-brain barrier typically precludes systemic delivery of large viral particles (although see (124)). We have recently described a parallel injector array that can deliver viruses into complex three-dimensional configurations (125). Finally, in utero electroporation of ChR2-GFP into embryonic mice at embryonic day ~15.5 has been found to label pyramidal cells selectively in layers 2/3 (53, 110).

Of potential interest is the possibility of a new generation of neural prosthetics, which can accomplish the synthetic neurobiology mission of repairing the nervous system by enabling optical input of information to sculpt neural dynamics and overcome pathology. To deliver these genes in a safe, efficacious, and enduring way, viruses such as AAV may be valuable; AAV has been used in over 600 human patients in gene therapy clinical trials without a single serious adverse event (126), and has been successfully used with opsin delivery. The ability to control specific targets optically within the brain may enable more potent and side-effect free therapies than possible with existing electrical and magnetic neuromodulation therapies, or with drugs that are often nonspecific and have side effects. Several groups have already prototyped blindness therapies that may enable new approaches to a currently intractable set of disorders, those in which photoreceptors degenerate within the retina (127, 128). To that end, the recent assessment of brain and immune function in nonhuman primates after ChR2 expression and activation, which showed a lack of harmful effects in a preliminary study (107), may pave the way towards new ideas for neural prosthetics for humans.

One strategy that has become widely popular is to inject the brain of a mouse expressing Cre recombinase in a specific cell type, with either a virus that bears an opsin preceded by a lox-flanked stop cassette, or a virus that bears an opsin reversed and flanked by pairs of lox sites in a specific configuration (Fig. 7; (108, 109)). Given the very large number of Cre transgenic mice in existence, and that are being generated, this strategy is likely to be very useful, at least for mice. Transgenic mice that express Cre in extremely



Fig. 7. Transgenic mouse expressing Cre within specific cells, coupled to lox-containing AAV viruses, enables cell typespecific opsin expression. (a) A pair of loxP recombination sequences meditate the removal of the transcriptional and translational stop cassette containing multiple poly-adenylation signals (STOP), in the presence of Cre (provided in transgenic mice within specific cell types), to initiate gene expression. (b) Two pairs of loxP-type recombination sequences (FLEX) for stable inversion proceed in two steps: (1) inversion followed by (2) excision. loxP and lox2272 are orthogonal recombination sites. (Adapted from (109) and (108)).

cell-specific ways (e.g., through 3' UTR knockins at the ends of cell type-specific genes) can be made, and then viruses can be rapidly made as new opsins are created, thus enabling cell type-specific expression without requiring the difficult process of trimming cellspecific promoters to fit within the small viral payload, or the difficult process of making transgenic mice for each new opsin tool that is developed (given the rapid pace of innovation, as shown in Sects. 1–4).

6. Hardware for Optical Neural Control

For in vitro use, xenon lamps (e.g., Sutter DG-4, Till Photonics Polychrome) equipped with fast-moving mirrors or monochromators can be used for flexible delivery of fast (millisecond timescale), bright light pulses to biological samples on microscopes. Fluorescence filters can be used to deliver light of the appropriate wavelength (e.g., GFP excitation filter for ChR2, rhodamine or Texas Red excitation filter for Arch, Texas Red excitation filter for Halo, and GFP or YFP excitation filter for Mac). Recently, many companies such as Thorlabs have begun to sell LEDs or LED arrays compatible with microscope fluorescence illuminators, which sell for a small fraction of the price of a full lamp setup. Or fiber-coupled LEDs can simply be placed nearby to the sample (129). Confocal and two-photon microscopes, or more generally scanning laser methodologies, can be used to drive opsins, as have been described in a variety of papers (110, 130, 131). Recently, digital micromirror displays (DMDs) have come forth as potentially useful for photostimulating in complex patterns, comprising millions of individual pixels that can be toggled either on or off (132, 133).

In vivo, the brain scatters light starting within a few hundred microns of an optical source, and absorbs light starting within a few millimeters of distance. Thus, most efforts for in vivo neuromodulation focus on delivering light to a volume of tissue, ranging from a very small volume containing a few hundred cells to a large volume (say, a few cubic millimeters) containing many thousands of cells. One widespread method is to use a laser coupled to an optical fiber (Fig. 8a shows a versatile setup that couples multiple colors of laser light into a single fiber; simpler commercially available single-color laser-coupled fibers with TTL control are also available), and to insert the fiber into a cannula implanted in the brain (Fig. 8b shows a hand-built one for mice; commercial versions from companies such as Plastics One can also be built) or directly into the brain (Fig. 8c shows a setup for monkey), or to couple the fiber to an implanted fiber via a ferrule. An optical commutator (e.g., from Doric Lenses) can be placed between the



Fig. 8. (a) Schematic design (*left*) and picture (*right*) of an optics assembly used to couple blue and yellow laser light into a single optical fiber for in vivo neural modulation. A pictured assembly, lacking a neutral density filter, shows the hardware laid out on a standard optical breadboard. (b) Schematic design (*left*) and picture (*right*) of a system for targeting and securing optical fibers within the brain. A polyimide cannula (1, 250 μ m ID), designed to terminate at the locus of optical modulation, is epoxied to a stack of hex nuts (2, sized 2–56) which will be secured to the skull with dental cement. Vented screws (3, sized 2–56), which have holes in their centers, screw into the nuts while leaving a path open to the cannula. A dummy wire (4, 230- μ m stainless steel wire) may be epoxied to rotate freely without vertical displacement by a plastic washer (6, homemade), which is epoxied to the fiber and sandwiched in between the vented screw above and the cannula below. (c) Apparatus for optical activation and electrical recording. Photograph, showing optical fiber (200- μ m diameter) and electrode (200- μ m shank diameter) in guide tubes. Adapted from (19).

fiber that inserts into the brain and the fiber that connects to the laser, to allow free rotation (65). Arrays of custom-targetable optical fibers, each coupled to a miniaturized light source (e.g., a raw die LED) and targeted to a unique target, will open up the ability to drive activity in complex 3D patterns, enabling the perturbation of complex-shaped structures as well as the ability to perturb targets in a patterned fashion (134, 135).

Aside from the key advantage of being able to manipulate a specific cell type, another key advantage of optical stimulation is the lack of electrical artifact compared to conventional electrical stimulation methods. However, despite the lack of electrical artifact, light does produce a voltage deflection when the electrode tip is illuminated (19, 136). For example, Fig. 9 shows traces recorded



Fig. 9. Voltage deflections observed on tungsten electrodes immersed in saline (**a**) or brain (**b**), upon tip exposure to 200ms blue-light pulses (**i**) or trains of 10-ms blue-light pulses delivered at 50 Hz (**ii**). Light pulses are indicated by *blue dashes*. Electrode data were hardware filtered using two data acquisition channels operating in parallel, yielding a lowfrequency component ("field potential channel") and a high-frequency component ("spike channel"). For the "spike channel" traces taken in brain (**b**), spikes were grouped into 100-ms bins, and then the binned spikes were displayed beneath corresponding parts of the simultaneously acquired "field potential channel" signal (59 and 53 repeated light exposures for **bi** and **bii**, respectively). (Shown are the spikes in eight such bins – the two bins before light onset, the two bins during the light delivery period, and the four bins after light cessation.) For all other signals shown, ten overlaid traces are plotted. Adapted from (19).

on a tungsten electrode in saline illuminated by a pulsed laser beam, as adapted from (19). This voltage deflection slowly evolved over many tens of milliseconds, and accordingly was only recorded when the electrode voltage filtered at 0.7-170 Hz to examine local field potentials (Fig. 9, top traces of each panel). This voltage deflection was not recorded when the electrode voltage was filtered at 250-8,000 Hz to detect spike signals (Fig. 9, bottom traces of each panel). When light illuminated parts of the electrode other than the tip, no artifact was recorded; only illumination of the tip-saline interface resulted in the voltage transient. This phenomenon is consistent with a classical photoelectrochemical finding, the Becquerel effect, in which illumination of an electrode placed in saline can produce a voltage on the electrode (137, 138). Consistent with the generality of the Becquerel effect as a property of electrode-electrolyte interfaces, this artifact is observed on various electrode materials, such as stainless steel, platinum-iridium, silver/silver chloride, gold, nichrome, or copper. Similar slowly evolving voltage deflections were observed when tungsten electrodes were used to record neural activity in the brain during optical stimulation. Because the optical artifact was slowly evolving over many tens of milliseconds, spike waveforms were detected

without corruption by the artifact. However, local field potentials and field oscillations, which reflect coherent neural dynamics in the range of Hertz to tens of Hertz, may be difficult to isolate from this Becquerel artifact using the electrodes tested here. Notably, we have not seen the artifact with pulled glass micropipettes (such as previously used in (3) and (12), or in the mouse recordings with pulled glass pipettes in (107)). Thus, for recordings of local field potentials and other slow signals of importance for neuroscience, hollow glass electrodes may prove useful.

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